

The Origins of fMRI Contrast in SPEN Imaging at Ultra High Magnetic Fields



E. SOLOMON, N. PYATIGORSKAYA, P. BENDEL, D. LE BIHAN, L. CIOBANU, L. FRYDMAN

NeuroSpin, CEA, Saclay, France; Weizmann Institute, Rehovot, Israel

BACKGROUND

We explore the features of spatiotemporal encoding (SPEN) in fMRI.

- SPEN is a new single-scan imaging scheme providing an alternative tool for fMRI, which is based on spatial- instead of frequency-encoding using frequency-swept (chirped) pulses [1] (Fig 1).

Advantages of SPEN over EPI at ultrahigh field :

- Higher immunity to B_0 -inhomogeneities and to chemical-shift offsets [2].
- Can be operated in fully refocused mode vis-à-vis T_2^* and/or T_2 effects [2, 3, 4].

Our investigation on activation detected by SPEN fMRI;

- As function of field strength: at preclinical high (7T) and ultra-high (17.2T) magnetic fields
- Obtaining artifact-free rat brain images with high spatial resolution.
- Modulating the T_2^* -weighted contribution with fully T_2^* -refocused (variant where each readout event coincides with its own TE, thereby all T_2^* contributions being absent) and non-fully-refocused acquisitions.
- Monitoring modulations imposed by T_1 effect s (in-flow) with field strength and TR.

MATERIALS & METHODS

- 2D SPEN images were obtained for 10 male Wistar rats at 17.2T and 7T on Bruker Avance III scanners using custom-written sequences.
- Anesthesia protocol: medetomidine the initial dose of 110 $\mu\text{g/kg}$ was followed, after 20 minutes, by administration of a continuous injection, gradually increasing from 100 $\mu\text{g/kg/h}$ to 300 $\mu\text{g/kg/h}$ within a 2-hour period;
- Electric stimuli: pulse duration 0.3 ms, frequency 7 Hz, current intensity 2.3mA.
- **Stimulation:** Block-design paradigm consisting of 5 blocks (30 s rest, 30 s forepaw electrical stimulation, separated with 10min rest between runs) (Fig 2)
- **Acquisition parameters:**
 - FOV: 2 cm x 2 cm, matrix size 100 x 100, slice thickness 1.2 mm, BW 400 kHz at 17.2T, 357 kHz at 7T.
 - GE EPI parameters: TE = 11 ms, TR = 1500 ms;
 - SPEN parameters: $T_{\text{acq}} = 25\text{ms}$, $T_{\text{exc+full-refocusing}} = 25\text{ms}$, $T_{\text{exc+non-refocused}} = 5\text{ms}$.
 - Slices: 3 coronal slices for EPI, including the primary and secondary somatosensory cortex. The most activated slice was chosen for 2D SPEN acquisition.
- **Post processing :**
 - In-house Matlab image-reconstruction algorithms based on super-resolution (SR) principles [5];
 - Statistical analyses: SPM 8 (slice-timing, motion correction and spatial smoothing, $p < 0.005$)

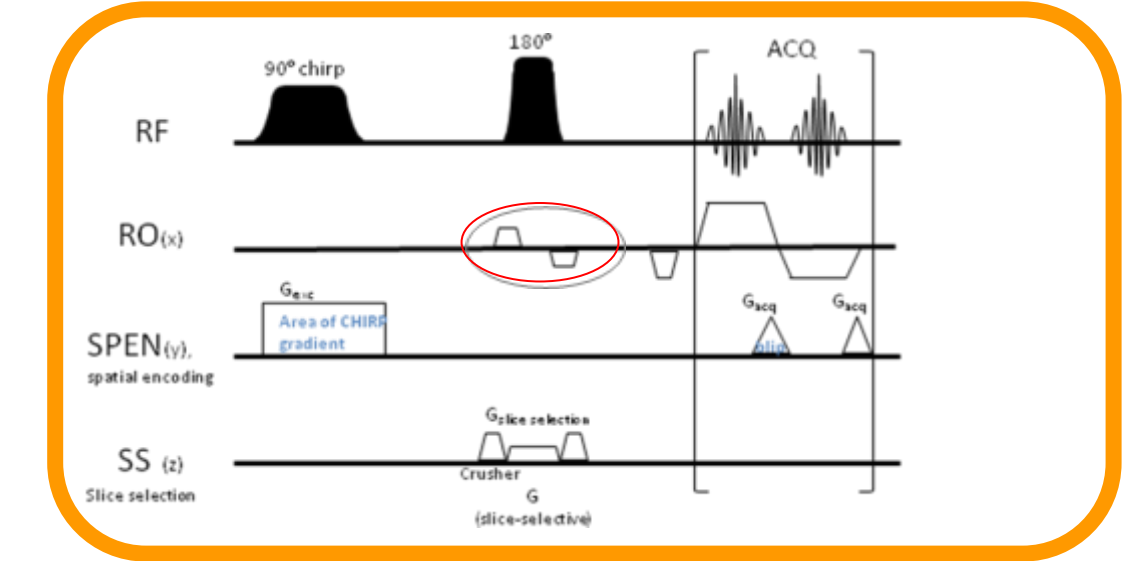


Figure 1. Spatio-temporal encoding (SPEN) single-scan 2D sequence, obtaining with spatial encoding and CHIRP pulse

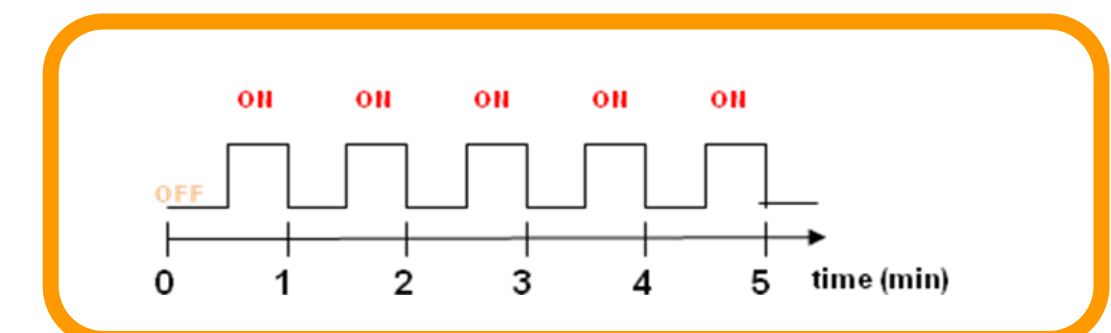


Figure 2. Stimulation paradigm

RESULTS

- At 17.2T: Fully refocused SPEN (TR = 1.5s): strong localized activation maps with good t-score levels (Fig. 3b).
- At 17.2T: Increasing TR from 1.5 s to 3 s: activation decreases (Fig. 3c).
- At 7T: the fMRI contrast in the fully refocused SPEN acquisitions decreases with field : For TR = 1.5 s the t-scores for SPEN were approximately three times smaller than for GE EPI.
- Switching from a fully T_2^* -refocused SPEN sequence, where $T_{\text{exc}} = T_{\text{acq}}$, to a non-refocused condition: classical T_2^* -driven BOLD contrast reinstated in SPEN, with very similar activation maps as in GE EPI(Fig 4c)

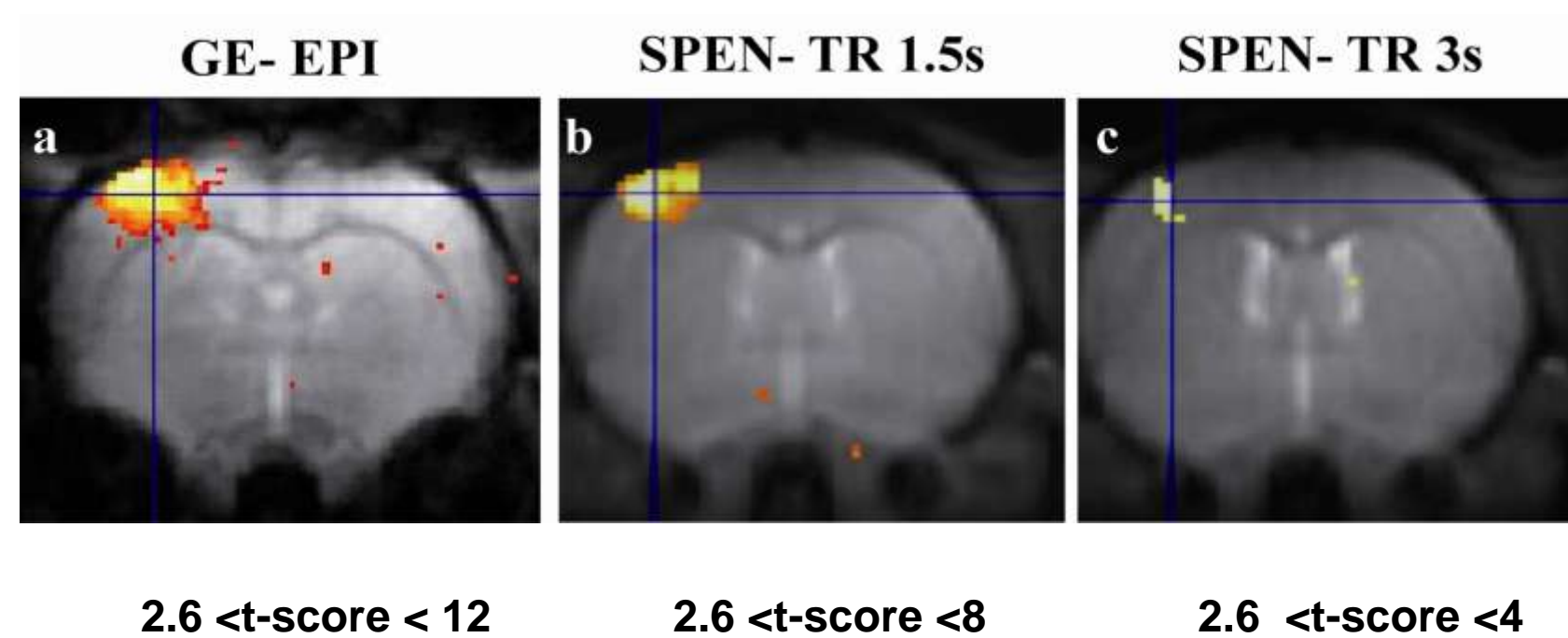


Figure 3: Comparison between GE EPI and SPEN fMRI maps recorded at 17.2 T. (a) GE- EPI; (b) fully T_2^* -refocused SPEN, TR 1.5s ;(c) fully T_2^* -refocused SPEN, TR 3s.

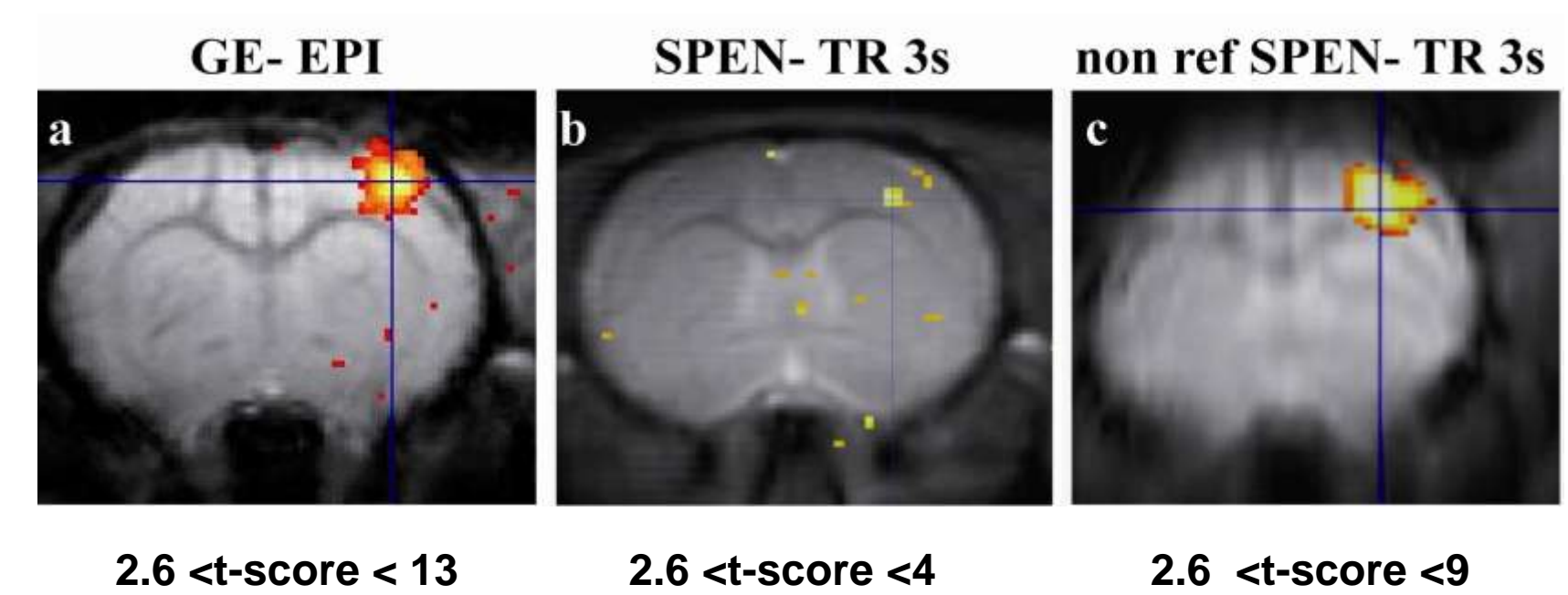


Figure 4: Comparison between GE-EPI, fully refocused and non-refocused SPEN fMRI maps recorded at 17.2 T. (a) GE- EPI; (b) fully refocused SPEN, TR 3s (c) non refocused SPEN, TR 3s.

DISCUSSION

- SPEN: method of choice for ultra-high magnetic field fMRI due to an enhanced robustness vis-à-vis field inhomogeneities and the chemical shift artifacts.
- TR signal dependence (Fig. 3) strongly suggests that T_1 -related effects contribute to the fMRI fully refocused SPEN. Further evidence of this T_1 contribution: at 7T, as T_1 gets shorter, fMRI enhancement decreases.
- Non-refocused SPEN allows strong fMRI signal enhancement –similar to classical T_2^* -driven BOLD contrast- while preserving good quality of image.
- Strong activation effects observed at very high fields in fully self-refocused mode can be related to in-flow and/or to T_2^* effects: possible variations of contrast as function of chosen sequence parameters

CONCLUSIONS

- fMRI SPEN: besides the T_2^* -weighted BOLD contribution in non-refocused sequences, signal contains a strong component caused by apparent T_1 -related in-flow effects.
- SPEN: very attractive and interesting tool to explore functional activation.

Acknowledgements: The authors thank Dr. Noam Ben-Eliezer for help in the initial stages of this work. This research was supported by the Minerva Foundation, a Helen and Kimmel Award for Innovative Investigation, the generosity of the Perlman Family Foundation, and the Laboratory of Integrative Biology and the Laboratory of Nuclear Magnetic Resonance (CEA).

References [1] Tal A and Frydman L, 2010, *Prog. NMR Spectrosc.*, 57, 241-292. [2] Ben-Eliezer N, Shrot Y and Frydman L, 2010, *Magn Reson Imag*, 28, 77-86. [3] Chamberlain R et al, 2007, *Magn Reson Med*, 58, 794-799. [4] Ben-Eliezer N., Goerke U., and Frydman L., *Proc. Intl. Soc. Mag. Reson. Med.* 19 (2011). [5] Ben-Eliezer N, Irani M, Frydman L, *Magn. Reson. Med.* (2010) 63, 1594–1600